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آموزش مهارت های کاربردی در تدوین و چاپ مقاله
Floating Matrix Tablets of Domperidone Formulation and Optimization Using Simplex Lattice Design

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Abstract

The purpose of this research was to prepare a floating matrix tablet containing domperidone as a model drug. Polyethylene oxide (PEO) and hydroxypropyl methylcellulose (HPMC) were evaluated for matrix-forming properties. A simplex lattice design was applied to systemically optimize the drug release profile. The amounts of PEO WSR 303, HPMC K15M and sodium bicarbonate were selected as independent variables and floating lag time, time required to release 50% of drug (t50) and 80% of drug (t80), diffusion coefficient (n) and release rate (k) as dependent variables. The amount of PEO and HPMC both had significant influence on the dependent variables. It was found that the content of PEO had dominating role as drug release controlling factor, but using suitable concentration of sodium bicarbonate, one can tailor the desired drug release from hydrophilic matrixes. The linear regression analysis and model fitting showed that all these formulations followed Korsmeyer and Peppas model, which had a higher value of correlation coefficient (r). The tablets of promising formulation were found to be stable for 3 months under accelerated (40°C/75% RH) stability testing.

Keywords: Domperidone; Floating matrix tablets; Simplex lattice design; Release kinetics; Polyethylene oxide; Hydroxypropyl methylcellulose; Floating lag time; Total floating time.

Introduction

Rapid gastrointestinal transit could result in incomplete drug release from the device above the absorption zone leading to diminished efficacy of the administered dose (1). Therefore, different approaches have been proposed to retain the dosage form in the stomach. These include bioadhesive systems, (2) swelling and expanding systems, (3, 4) and floating systems (5, 6). Large single-unit dosage forms undergo significant swelling after oral administration and the swollen matrix inhibits the gastric emptying even at an uncontractile state of the pyloric sphincter. Park and Park reported medicated polymeric sheets and swelling of balloon hydrogels (7). But the swelling and expanding systems may show the hazard of permanent retention. Bioadhesive systems may cause problems such as irritation of the mucous layer owing to high localized concentration of the drug (8). Hydrodynamically balanced systems were designed using effervescent mixtures.

In recent years, polyethylene oxide (PEO) has attracted much attention as a polymeric excipient that can be used in formulations for different purposes. For instance, formulations with PEO have been extruded to make different products such as swellable and erodible implants.
(9), scaffolds for tissue engineering (10), or, to be used in the production of micelles with amphiphilic drugs, when solid dispersions incorporating these drugs are placed in aqueous environments (11). However, PEOs are mostly used to produce controlled release solid dosage forms such as matrixes, reservoirs, or coated cores (12, 13, 14). Due to their chemical structure, PEOs are among various hydrophilic polymers that, in the presence of water, control the release of the active moiety either by swelling (large molecular weight; > 2 MDa (mega Dalton)) or by eroding and swelling (small molecular weight; < 0.9 MDa), forming a hydrogel. In both cases, water triggers the process starting the erosion and/or the swelling processes. All this attention to PEOs is due to the consequential of their physical and chemical stability, compressibility, high swelling ability, and good solubility in water. Thus, PEOs have been proposed as alternatives to cellulose or other ethylene glycol derivatives in the production of tablets or granules.

Domperidone is a synthetic benzimidazole compound that acts as a dopamine D2 receptor antagonist. Its localization outside the blood-brain barrier and antiemetic properties have made it a useful adjunct in therapy for Parkinson’s disease. There has been renewed interest in antidopaminergic prokinetic agents since the withdrawal of cisapride, a 5-HT4 antagonist. Domperidone was a kind gift from Maan Pharmaceutical Ltd (Mehsana, India). Polyethylene oxide WSR 303 (Polyox® WSR 303, mw = 7×10^6) was received as a gift sample from Dow Chemical Company, New Jersey (USA), Hydroxypropyl methylcellulose (HPMC K15 M), and sodium bicarbonate were procured from Laser Chemicals (Ahmedabad, India). Magnesium stearate and talc were purchased from Apex Chemicals (Ahmedabad, India). All other ingredients used were of analytical grade and were used as received.

Methods
Preparation of domperidone floating tablets Domperidone, the required quantity of polymers (Polyox® WSR 303 and HPMC K15M), sodium bicarbonate and starch were mixed in mortar by spatula for 15 min. The powder blend was then lubricated with talc and magnesium stearate and compressed in tablets using 8 mm flat-face round tooling on rotary tablet press (Rimek, India, Ahmedabad). Compression force was adjusted to obtain tablets with hardness in range of 4.5 Kg/cm^2. The tablets weighed 145 ± 2 mg, had a round flat-face with average diameter 8 ± 0.1 mm and a thickness of 2.5 ± 0.2 mm.

Simplex lattice design
A simple lattice design (21) was adopted to optimize the formulation variables. In this design, three factors were evaluated by changing their concentrations simultaneously to optimize the formulation variables. In this experiment, statistical model incorporating 7 interactive terms was used to evaluate the responses.

<table>
<thead>
<tr>
<th>Batch Code</th>
<th>X1</th>
<th>X2</th>
<th>X3</th>
<th>FLT ± SD (sec)</th>
<th>t50% ± SD (h)</th>
<th>t80% ± SD (h)</th>
<th>n ± SD</th>
<th>k ± SD</th>
</tr>
</thead>
<tbody>
<tr>
<td>S1</td>
<td>1</td>
<td>0</td>
<td>0</td>
<td>20 ± 2</td>
<td>9.03 ± 1.9</td>
<td>12.34 ± 2.2</td>
<td>0.73 ± 0.045</td>
<td>6.44 ± 0.3</td>
</tr>
<tr>
<td>S2</td>
<td>0</td>
<td>1</td>
<td>0</td>
<td>55 ± 3</td>
<td>12.68 ± 2.3</td>
<td>17.45 ± 2.6</td>
<td>0.59 ± 0.007</td>
<td>9.83 ± 1.2</td>
</tr>
<tr>
<td>S3</td>
<td>0</td>
<td>0</td>
<td>1</td>
<td>10 ± 4</td>
<td>11.70 ± 0.8</td>
<td>21.57 ± 0.8</td>
<td>0.62 ± 0.0046</td>
<td>9.920 ± 0.4</td>
</tr>
<tr>
<td>S4</td>
<td>0.5</td>
<td>0.5</td>
<td>0</td>
<td>35 ± 5</td>
<td>17.07 ± 1.7</td>
<td>26.35 ± 1.0</td>
<td>0.53 ± 0.032</td>
<td>14.45 ± 2.1</td>
</tr>
<tr>
<td>S5</td>
<td>0</td>
<td>0.5</td>
<td>0.5</td>
<td>98 ± 3</td>
<td>18.11 ± 1.4</td>
<td>28.49 ± 1.1</td>
<td>0.48 ± 0.019</td>
<td>15.40 ± 0.3</td>
</tr>
<tr>
<td>S6</td>
<td>0.5</td>
<td>0</td>
<td>0.5</td>
<td>25 ± 2</td>
<td>11.94 ± 0.5</td>
<td>23.81 ± 0.7</td>
<td>0.63 ± 0.021</td>
<td>13.38 ± 0.7</td>
</tr>
<tr>
<td>S7</td>
<td>0.33</td>
<td>0.33</td>
<td>0.33</td>
<td>39 ± 3</td>
<td>15.27 ± 1.2</td>
<td>23.07 ± 2.0</td>
<td>0.57 ± 0.002</td>
<td>12.39 ± 1.8</td>
</tr>
</tbody>
</table>

The simplex lattice design for a 3-component system is represented by an equilateral triangle in 2-dimensional space (Figure 1). Seven batches (S1-S7) were prepared (Table 1) by taking three independent variables; one at each vertex (X1, X2, X3), one at the halfway point between vertices (X1X2, X2X3, X3X1), and one at the center point (X1X2X3). Each vertex represents a formulation containing the maximum amount of 1 component, with the other 2 components at a minimum level. The halfway point between the 2 vertices represents a formulation containing the average of the minimum and maximum amounts of the 2 ingredients represented by 2 vertices. The center point represents a formulation containing one third of each ingredient.

The amounts of matrixing agent (Polyethylene oxide WSR 303, X1) gelling agent, (HPMC K15 M, X2) and gas-generating agent (sodium bicarbonate, X3) were selected as independent variables. Floating lag time (FLT), time required for 50% and 80% drug dissolution; n: Diffusion coefficient; k: Release rate constant; X1: Amount of Polyethylene oxide WSR 303 (mg); X2: Amount of HPMC K15 M (mg); X3: Amount of Sodium bicarbonate (mg). All batches contained 30 mg of domperidone, 20 mg of maize starch, 2% w/w of talc, and 1% w/w of magnesium stearate. Average weight of each tablet was 145 mg.

Figure 1. Equilateral triangle representing simplex lattice design for 3 components.
is the estimated coefficient for the factor \(X_i\). The main effects (\(X_1, X_2,\) and \(X_3\)) represent the average result of changing 1 factor at a time from its low to high value. The interaction terms (\(X_1X_2, X_1X_3, X_2X_3,\) and \(X_1X_2X_3\)) show how the response changes when 2 or more factors are simultaneously changed. The statistical analysis of the simplex lattice design batches was performed by multiple linear regression analysis using Microsoft Excel.

In-vitro buoyancy studies

The in-vitro buoyancy was determined by floating lag time as per the method described by Rosa et al. (22). The tablets were placed in a 100 mL glass beaker containing simulated 0.1 N Hydrochloric acid, as per USP. The time required for the tablet to rise to the surface and float, was determined as the floating lag time.

In-vitro dissolution studies

The in-vitro dissolution study of domperidone tablets was performed using USP apparatus (model TDT-06T, Electrolab, Mumbai, India) fitted with paddles (50 rpm) at 37°C ± 0.5°C using Hydrochloric acid (pH 1.2, 900 mL) as a dissolution medium. At the predetermined time interval, 5 mL samples were withdrawn, filtered through a 0.45 μm membrane.

Calculation of immediate release part

The pharmacokinetic parameters of domperidone were used to calculate a theoretical drug release profile for a 24 h dosage form. The immediate release part for sustained release domperidone was calculated using Equation 1 and was found to be 4.211 mg.

\[
\text{Immediate release part} = \left(\frac{C_{ss} - V_D}{F}\right)
\]

Where, \(C_{ss}\) is steady-state plasma concentration (Average \(C_{max}\)), \(V_D\) is volume of distribution, and \(F\) is fraction bioavailable.

Calculation of diffusion exponent \(n\)

Hence, the formulation should release 4.211 mg up to 24 h. Hence, it was decided to optimize HPMC K 15 M for drug, HPMC K 15 M in a 1:1 ratio HPMC K15M might not achieve low floating lag time. Below drug to ratio, the floating lag time increased, indicating that a high amount of HPMC is undesirable to achieve low floating lag time. Below drug to polyethylene oxide WSR 303 ratio, the floating lag time decreased, indicating that a high amount of HPMC is desirable to achieve low floating lag time.

**Results and Discussion**

Polyethylene oxide WSR 303 was selected as a matrixing agent to impart sufficient integrity of the tablets. HPMC K 15 M was selected as a gelling agent, considering its widespread applicability and excellent gelling activity in sustained release formulations. Sodium bicarbonate was optimized as CO₂ producing agent from preliminary studies. HPMC K 15 M in a 1:1 ratio. Twenty mg of sodium bicarbonate was optimized as CO₂ producing agent from preliminary studies. The values for Floating lag time (FLT), time required for 50% and 80% drug release (t 50% and t 80% respectively), release rate constant (k) and diffusion component (n) for all 7 batches were given in Table 2. The data clearly indicate that the values of FLT, t 50%, t 80%, k and n are strongly dependent on the selected independent variables.

Dissolution profiles of all batches of factorial design were compared with theoretical data clearly indicate that the values of FLT, t 50%, t 80%, k and n are strongly dependent on the selected independent variables.
dissolution profile. The results of similarity factor indicate that batches S’ to S’5 fulfill the above criteria. But batch S, showed highest f2 among all the batches. Hence, batch S, more similar compare to other batches of simplex lattice design, similarity between theoretical dissolution profile and dissolution profile of S, is shown in Figure 3.

The fitted equation relating the responses Floating lag time (FLT), time required for 50% and 90% drug release (t50% and t90%, respectively), release rate constant (k) and diffusion component (n) to the transformed factor are shown in Equations 2, 3, 4, 5 and 6, respectively.

\[ FLT = 98.7859 \times 0.62.4770 \times X_1 - 87.4770 \times X_2 - 62.7759 \times X_3 - 132.7759 \times X_4 \times X_5 \]
\[ R\text{-square}=0.98263 \]  
Equation 2

\[ t_{50\%} = 12.4872 - 1.2714 \times X_1 + 9.6857 \times X_3 - 5.9428 \times X_1 \times X_3 \]
\[ R\text{-square}=0.90511 \]  
Equation 3

\[ t_{90\%} = 19.1078 + 17.2948 \times X_1 \]
\[ R\text{-square}=0.9418883 \]  
Equation 4

\[ n = 0.6422 + 0.0676 \times X_1 - 0.6017 \times X_3 - 0.4456 \times X_3 \]
\[ R\text{-square}=0.9722806 \]  
Equation 5

\[ k = 9.0676 + 22.9004 \times X_1 - 24.8700 \times X_3 \]
\[ R\text{-square}=0.9180772 \]  
Equation 6

The high value of correlation coefficient for FLT, t50%, t90%, n and k indicate good fit (Table 2). The polynomial equations can be used to draw the conclusions after considering the magnitude of coefficient and the mathematical sign that it carries (i.e., positive or negative).

Tablets of all batches (S, to S,5) had floating lag time varies from 10 sec to 98 sec. Polynomial equation for floating lag time (Equation 2) suggests that the amount of PEO WSR 303 (X1), HPMC K 15 M (X2) and amount of sodium bicarbonate (X3) are strongly dependent on floating lag time. The high value of X1 coefficients also suggests that the interaction between X1 and X3 has a significant effect on FLT. It can be concluded that the FLT changed by appropriate selection of the X1 and X3 levels.

The time required to release 50% of drug (t50%) and the time required to release 80% of drug (t90%) showed wide variation (Table 1). Figures 5 and 6 show the 3D surface plot of the amount of PEO WSR 303 (X1), HPMC K 15 M (X2) and sodium bicarbonate (X3) versus t50% and t90%, respectively. The data clearly indicate that the dependent variables (t50%, t90%, n) are strongly dependent on the independent variables. The fitted equation relating the response t50% and t90%, to the transformed factors are shown in Equations 3 and 4. Data of t50% and t90% clearly indicate that increase in the amount of sodium bicarbonate leads to decrease in the time required to 50% drug release. It may due to pores formation in tablet by sodium bicarbonate which produce CO2 when interacts with dissolution medium. The high value of X1, X2 coefficient also suggests that the interaction between X1 and X2 has a significant effect on t90%. It can be concluded that the t90% changed by an appropriate selection of the X1 and X2 levels.
Dissolution profiles were fitted with the power law equation given by Korsmeyer and Peppas\(^6\). Diffusion exponent value varies from 0.489 to 0.7332 indicate that drug release pattern anomalous involves the combination of swelling, diffusion and/or erosion of matrices. This might be due to the poor water solubility of domperidone as well as the difference exists in characteristics of polymers. Non-linear relationship was obtained between the amount of PEO WSR 303 (X1), HPMC K 15 M (X2) and sodium bicarbonate (X3) versus release rate constant (k).

Release rate constant showed that independent factors had significant influence (p < 0.05). The high value of X1, X2 and X3 coefficient also suggests that the interaction between X1, X2 and X3 has a significant effect on release rate constant. It can be concluded that the release rate constant changed by appropriate selection of the X1, X2 and X3 levels. Figure 8 shows the 3D surface plot of the amount of PEO WSR 303 (X1), HPMC K 15 M (X2) and sodium bicarbonate (X3) versus diffusion exponent. The amount of PEO and HPMC both had a dominating role as drug release controlling factor, but using suitable concentration of sodium bicarbonate, one can tailor the desired drug release from hydrophilic matrices for the development of floating tablets.

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**References**


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